

See discussions, stats, and author profiles for this publication at: <https://www.researchgate.net/publication/344444553>

Voice Quality Evaluation in Patients With COVID-19: An Acoustic Analysis

Article in *Journal of Voice* · October 2020

DOI: 10.1016/j.jvoice.2020.09.024

CITATIONS

3

READS

254

5 authors, including:



Maral Asiaee

Alzahra University

14 PUBLICATIONS 5 CITATIONS

[SEE PROFILE](#)



Amir Vahedian Azimi

Baqiyatallah University of Medical Sciences

110 PUBLICATIONS 709 CITATIONS

[SEE PROFILE](#)



Abdalsamad Keramatfar

Academic Center for Education, Culture and Research

53 PUBLICATIONS 62 CITATIONS

[SEE PROFILE](#)



Mandana Nourbakhsh

Alzahra University

42 PUBLICATIONS 48 CITATIONS

[SEE PROFILE](#)

Some of the authors of this publication are also working on these related projects:



CORONA Research [View project](#)



Morphology [View project](#)

Voice quality evaluation in patients with COVID-19: An acoustic analysis

Maral Asiaee , Amir Vahedian-azimi , Seyed Shahab Atashi ,
Abdalsamad Keramatfar , Mandana Nourbakhsh

PII: S0892-1997(20)30368-4
DOI: <https://doi.org/10.1016/j.jvoice.2020.09.024>
Reference: YMVJ 3014



To appear in: *Journal of Voice*

Accepted date: 29 September 2020

Please cite this article as: Maral Asiaee , Amir Vahedian-azimi , Seyed Shahab Atashi , Abdalsamad Keramatfar , Mandana Nourbakhsh , Voice quality evaluation in patients with COVID-19: An acoustic analysis, *Journal of Voice* (2020), doi: <https://doi.org/10.1016/j.jvoice.2020.09.024>

This is a PDF file of an article that has undergone enhancements after acceptance, such as the addition of a cover page and metadata, and formatting for readability, but it is not yet the definitive version of record. This version will undergo additional copyediting, typesetting and review before it is published in its final form, but we are providing this version to give early visibility of the article. Please note that, during the production process, errors may be discovered which could affect the content, and all legal disclaimers that apply to the journal pertain.

© 2020 The Voice Foundation. Published by Elsevier Inc. All rights reserved.

Voice quality evaluation in patients with COVID-19: An acoustic analysis

Maral Asiaee

Department of Linguistics, Faculty of Literature, Alzahra University, Tehran, Iran.

m.asiaee@alzahra.ac.ir

Amir Vahedian-azimi

Trauma research Center, Nursing Faculty, Baqiyatallah University of Medical Sciences, Tehran, Iran.

Amirvahedian63@gmail.com

Seyed Shahab Atashi

Department of Food and Drug control, Jundishapour University of Medical Sciences, Ahvaz, Iran

seyedshahabatashi@gmail.com

Abdalsamad Keramatfar

Department of Data Analytics, Scientific Information Database (SID), Tehran, Iran.

samad@sid.ir

Mandana Nourbakhsh (Corresponding Author)

Department of Linguistics, Faculty of Literature, Alzahra University, Tehran, Iran.

nourbakhsh@alzahra.ac.ir

North Sheikh Bahae St., Deh-e Vanak, Tehran, I. R. of Iran.

P. Code: 1993891176

Voice quality evaluation in patients with COVID-19: An acoustic analysis

Abstract

Objectives. With the COVID-19 outbreak around the globe and its potential effect on infected patients' voice, this study set out to evaluate and compare the acoustic parameters of voice between healthy and infected people in an objective manner.

Methods. Voice samples of 64 COVID-19 patients and 70 healthy Persian speakers who produced a sustained vowel /a/ were evaluated. Between-group comparisons of the data were performed using the two-way ANOVA and Wilcoxon's rank-sum test.

Results. The results revealed significant differences in CPP, HNR, H1H2, F0SD, jitter, shimmer and MPT values between COVID-19 Patients and the healthy participants. There were also significant differences between the male and female participants in all the acoustic parameters, except jitter, shimmer and MPT. No interaction was observed between gender and health status in any of the acoustic parameters.

Conclusion. The statistical analysis of the data revealed significant differences between the experimental and control groups in this study. Changes in the acoustic parameters of voice are caused by the insufficient airflow, and increased aperiodicity, irregularity, signal perturbation and level of noise, which are the consequences of pulmonary and laryngological involvements in patients with COVID-19

Keywords: Coronavirus disease, covid-19 patients, voice quality, acoustic analysis

1. Introduction

In early March 2020, the World Health Organization (WHO) declared COVID-19, as a pandemic. Since then, with more than 17,000,000 confirmed cases worldwide and counting, coronavirus has become one of the most challenging issues with which the world is faced. As indicated by Rothan and Byrareddy¹, COVID-19 principally affects the respiratory system, and people infected with the disease may experience pneumonia and acute respiratory distress syndrome. Symptoms of acute upper respiratory tract infections, such as cough, sore throat, rhinorrhea and sneezing, as well as digestion symptoms, like vomiting, are associated with mild cases of this disease, and symptoms like pneumonia and acute respiratory distress are primarily seen in severe and critical cases, respectively.² “Respiratory tract infections affect the same system and structure that are used for voice production”.³ Although the primary function of the respiratory tract is to provide oxygen to the body, its secondary and equally important function is to provide energy and produce phonation for the purpose of speech communication.

Voice production is a 3-stage process: Respiration, phonation and resonating system. In the respiratory stage, the force that is needed for generating sound is provided by the air expelled from the lungs. A person who has contracted the coronavirus not only may experience shortness of breath but may also have difficulty exhaling, which results in the lack of energy to produce sound and hence a disruption in the speech production cycle. In the phonation stage, the subglottal pressure must reach a certain point to set the vocal folds into a vibratory position. If the first stage of speech mechanism is disrupted, the phonation function of the larynx will be accordingly impaired. Other symptoms of coronavirus, such as recurrent dry coughs, may cause changes in the vocal folds and will consequently give rise to modifications in the acoustic cues related to voice quality. As shown in a study using self-assessment questionnaires, 28.6% of those infected with COVID-19, showed symptoms of dysphonia.⁴ Nonetheless, using only self-assessed results is subjective and prone to error.

The acoustic analysis of voice quality is of great interest among phoneticians and voice clinicians due to its noninvasive nature, low costs and ease of application.^{5,6,7} In 2001, the European Laryngological Society (ELS) put forward a basic protocol for assessment of voice-related diseases in which they recommended using the acoustic analysis of speech as a diagnostic tool.⁷ In the ELS protocol, fundamental frequency (F0), perturbation measures of pitch (jitter) and amplitude (shimmer) as well as harmonic-to-noise ratio (HNR) were noted as relevant parameters when evaluating voice quality.⁷ Along with these parameters, which are the most frequently-used ones^{6,8,9}, cepstral peak prominence (CPP)^{10,11,9,12,13}, harmonic amplitude measures^{14,15} and the aerodynamic parameter of voicing, i.e. maximum phonation time (MPT)^{16,17} are among the most-studied characteristics of voice. In addition to all the aforementioned parameters, this study also employed fundamental frequency variation (F0 standard deviation) and number of voice breaks (NVB) for accomplishing the study objective.

Fundamental frequency is the rate at which vocal folds vibrate per second and is expressed in Hertz (Hz). Changes in mass, length and tension of the vocal folds modify the fundamental frequency.^{18, 19, 20} Variation in fundamental frequency is either normal (e.g. difference between F0 in children, women and men) or may occur because of vocal fold pathologies.²¹ Asymmetrical changes in the mass and tension of the vocal folds caused by a laryngeal pathology such as tumors or paralysis lead to a deviant vibration and consequently change the fundamental frequency.²² F0SD depicts the amount of variation in the frequency of vocal fold vibration.²³

Jitter and shimmer are defined as the cycle-to-cycle variation in frequency and amplitude during phonation, respectively.²¹ Normally, in healthy speakers, vibration of vocal folds show a low-level jitter, and higher levels of jitter are observed in pathological voices.²⁴ Variation in shimmer is mostly detected when there is a mass lesion in the vocal folds such as edema, polyps or carcinomas.²⁵ Values above 1.04% for jitter and above 3.81% for shimmer in adult speakers are considered pathological.²⁶

HNR, also known as signal-to-noise ratio, depicts the degree of periodicity in a signal.²⁷ It is an estimate of energy in the harmonics of voice signal and the noise energy in the signal.²¹ HNR values are usually higher in normal voice than in pathological voice, since normal voices are more sonorant than pathological ones. HNR values below 7dB are stated to be pathological.^{28,29}

CPP is another measure that corresponds to the degree of regularity and periodicity of the voice signal.²⁷ Derived via linear regression, CPP gauges “the relative amplitude of the cepstral peak prominence in relation to the expected amplitude”.^{14,30} Dysphonic voices show lower CPP values in comparison to normal voices, which exhibit higher level of CPP.¹⁰

Difference between the amplitude of the first and second harmonics (H1-H2) is indicative of the degree of glottal adduction in different voices.³¹ As this parameter reflects changes in the open quotient, the higher is the value of (H1-H2), the greater is the open quotient. The (H1-H2) measure is associated with breathiness in the voice. Breathy voices show higher (H1-H2) values; however, strained voices exhibit lower (H1-H2) values.³²

In Praat³³, the number of voice breaks (NVB) is defined as “the number of distances between consecutive pulses that are longer than 1.25 divided by the pitch floor”. It is believed that normal voices show a lower number of voice breaks than pathological voices.

MPT is an aerodynamic parameter that describes the maximum length with which a vowel can be vocalized continuously and is expressed in second.¹⁶ Generally, phonation time less than 10 seconds are considered abnormal.³⁴

Since COVID-19 is mostly considered as a respiratory disease, and many of its symptoms are associated with the larynx and the lungs infections, those acoustic parameters that represent these organs' functions, are chosen to be analyzed. Differences in the acoustic parameters of voice between patients and healthy participants could be considered as one of the diagnostic tools,

which depicts the involvement of the larynx and the other respiratory organs; hence, this study compares COVID-19 patients with healthy individuals to evaluate the effect of this disease on the noted acoustical parameters without resorting to invasive methods.

2. MATERIAL AND METHODS

The National Institute for Medical Research Development (NIMAD) Ethics Committee in Iran approved the study protocol under the code IR.NIMAD.REC.1399.056. All the participants had given their informed consent to use their speech samples for research purposes.

The present study was an observational case-control study.

2.1 Participants

Simple random sampling method was employed to choose the healthy participants. Patients were chosen from those people who were hospitalized at the Baqiyatallah hospital. Diagnosis of participants with COVID-19 was carried out using the World Health Organization (WHO) interim guidance.³⁵ Upon admission, chest computed tomographic (CT) scan plus swab test was performed for patients. Since the scan results are readily available (compared with the swab test which takes at least 24 hours), diagnosis was made based on the CT results; Moreover, positive results on a reverse-transcriptase polymerase chain reaction (PT-PCR) assay of a specimen obtained on a nasopharyngeal swab, indicated the confirmation of COVID-19. Therefore, all patients in this study, were positive based on the two methods.

At the initial stage of sampling, data from 100 healthy participants and 100 individuals with COVID-19 was collected. All these participants completed a questionnaire. The questionnaire contains questions about participants' gender, age, health background (including questions about any history of asthma, COPD, laryngitis and chronic bronchitis), their smoking habits, whether they have any history of substance abuse, whether the participants recently travelled during the COVID-19 pandemic and whether the participants were/are in contact with someone who was/is tested positive for COVID-19.

The inclusion criteria for the healthy participants was to be a non-smoker and non-drug addict, someone who did not travel during the pandemic and had/ has no contact with a person who has contracted COVID-19, in addition to having no prior voice disorder or any kind of respiratory disease. The inclusion criteria for patients were the same as healthy participants except for the travelling and being in contact with a COVID-19 patient.

The final number of participants who met the inclusion criteria was 147. Participants were then divided into an experimental and a control group. In the experimental group, speech samples of 77 speakers who had the disease were initially collected, but, after the first recording session, 13 patients were either transferred to the ICU or passed away. The final number of participants

whose data were used in the experimental group was thus 64 (38 male, 26 female). Their age ranged between 16 and 77 (mean= 52.3 years, SD= 12.89).

The control group comprised of 70 (33 male and 37 female) healthy Persian speakers who were aged 18 to 70 (mean=42.35 years, SD= 10.01).

2.2 Voice recordings

All recordings were obtained using ZOOM H5 handy recorder with a sampling rate of 44100 Hz and 16 bit quantization. During the recordings, the recorder was held at the distance of 20 cm with a 45° angle from the participants' mouth. Before starting the main recording sessions, the examiners demonstrated the task individually for each participant. To minimize the effect of intonational changes and any irregularity caused by the coarticulation effect, only a prolonged vowel was used.³⁶ All the participants were asked to produce a vowel, namely /a/, in as long a time as they could, at their comfortable pitch and with a flat tone and a constant amplitude. For the MPT assessment, the participants were asked to take a deep breath before producing the /a/ sound.

Two sessions of recording were carried out for each participant. In the control group, the recordings were carried out on two different sessions. In the experimental group, the interval between recordings was two days. The first recording was recorded on the day the participants were hospitalized and the second one, two days after their first recording session.

Voice recordings were done by two hospital nurses who were trained to do the speech data collection. All safety measures were taken by these nurses while recording; they wore face mask and face shield, disposable gloves and suits. The recorder was also sterilized before and after each recording session, using alcohol pads.

2.3 Parameter extraction

Two different methods were used for extracting the acoustical parameters related to voice quality. A Praat³³ script was used to extract the local values of jitter, shimmer, MPT and the number of voice breaks. The measurements were performed using the default settings in Praat. Fundamental frequency, CPP, HNRs and (H1-H2) were automatically extracted using VoiceSauce³⁷, a freeware for voice analysis. F0 measurement was done using the default algorithm of VoiceSauce, i.e. STRAIGHT.³⁸ By default, VoiceSauce detects F0 at 1-ms intervals and computes the harmonic spectra magnitude, pitch-synchronously over a three-cycle window; however, the default was changed into 5-ms intervals. In VoiceSauce, CPP is calculated using the algorithm proposed by Hillenbrand et al.¹⁴ HNR values are gauged using a variable window of five pitch periods by de Krom's algorithm.³⁹ HNR05, HNR15, HNR25, HNR35 measure HNR from 0-500 Hz, 0-1500 Hz, 0-2500 Hz and 0-3500 Hz, respectively. This study used HNR35 (henceforth HNR). Finally, H1*-H2* was used for (H1-H2) assessment, which is the H1-H2

corrected for the effect of formants based on the algorithm proposed by Iseli et al.⁴⁰ and used in VoiceSauce.

2.4 Statistical analysis

Data were analyzed in R (R Core Team 2020) version 4.0.0.⁴¹ Due to the large number of tokens extracted from the acoustic analysis of the parameters in VoiceSauce (F0, CPP, HNR and H1-H2), the average of the results for each parameter and each participant was first calculated. Two values were thus obtained for each parameter, each representing the value of that parameter in a repetition for each participant. Another averaging process was then carried out on the results obtained from all the parameters' repeated recordings; thus, for each participant and each parameter, only one value was obtained.

A two-way ANOVA was performed to evaluate the effects of participants' health status (healthy/sick (infected)) and gender (male/female) on the different acoustic parameters studied in this research. The data collected on the F0, CPP, HNR, H1H2 parameters were normally distributed according to Shapiro-Wilk's test of normality ($p > 0.05$). To evaluate the homogeneity of variances, Levene's test of homogeneity of variances was run. The assumption of homogeneity of variances was met ($p > 0.05$). Since data in jitter, shimmer, MPT and F0SD did not show a normal distribution, the nonparametric Wilcoxon rank-sum test was used. As for the number of voice breaks, only a descriptive analysis will be reported.

Figure 1. exhibits the data distribution for all the parameters across the different genders and for the different health status.

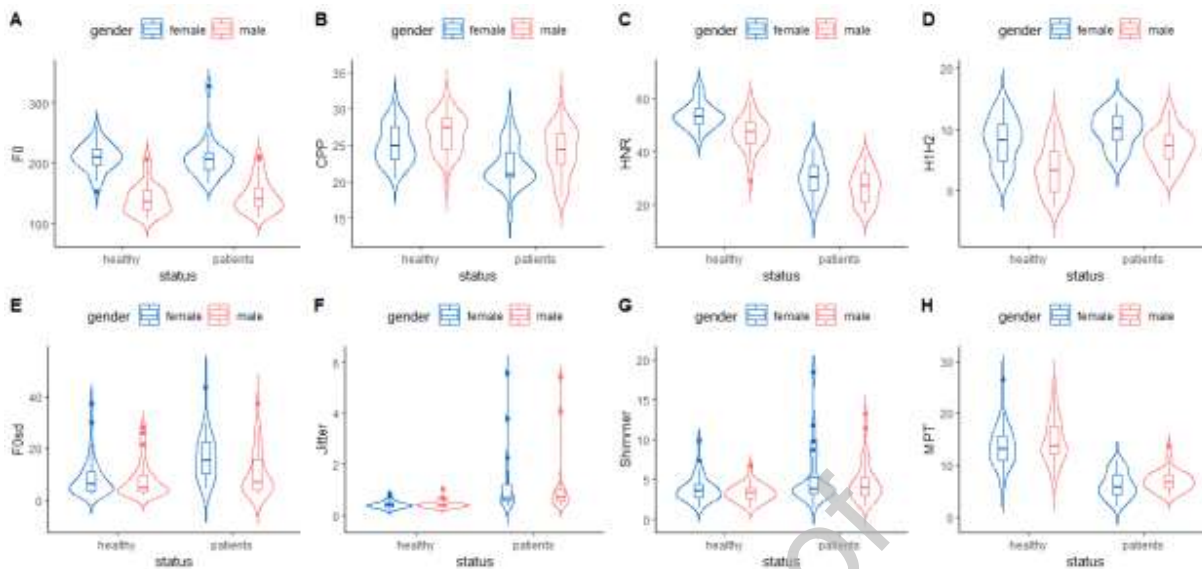


Figure 1.

Violin plot of the distribution of different acoustic parameters of voice in male and female participants categorized by their health status. The parameters represented in figures A-D in the first row were normally distributed, and the parameters represented in figures E-H in the second row were not normally distributed. Abbreviations: fundamental frequency (F0), cepstral peak prominence (CPP), harmonics-to-noise ratio (HNR), difference between the first and second harmonic amplitude (H1H2), standard deviation of fundamental frequency (F0SD) and maximum phonation time (MPT).

3. Results

Table 1 summarizes the total number of voice breaks (NVB) in the female and male participants grouped by their health status and across the two repetitions.

Table 1:
The descriptive analysis of the number of voice breaks

Gender	Health status	Voice break	Number	Percent	Summary
female	healthy	0	57	77	77 %
		1-2	17	23	23 %
		3-5	0	0	
		>6	0	0	
	patient	0	25	48.1	48.1 %
		1-2	19	36.5	51.9 %
		3-5	6	11.5	
		>6	2	3.9	
male	healthy	0	47	71.6	71.2 %
		1-2	17	25.8	28.8%
		3-5	1	1.5	
		>6	1	1.5	
	patient	0	39	51.3	51.3%
		1-2	27	35.5	48.7%
		3-5	5	6.6	
		>6	5	6.6	

Based on the data in Table 1, there was no voice break in 77% of the voice samples from the healthy female participants; as for the healthy male participants, the rate was 71.2%.

In the healthy groups, at least one voice break was observed in 23% of the women's and 28.8.9% of the men's phonation. The percentage of non-occurrence of voice breaks dropped to 48.1% for the female and 51.3% for the male patients in the COVID-19 group. A total of 51.9 % of the data from the women and 48.7% of the data from the men in the patients' group showed at least one voice break during the articulation of the sustained vowel /a/. Overall, the percentage of NVB was higher in them in comparison with the healthy participants.

Table 2 presents the mean, standard deviation and range of all the acoustic parameters in the healthy and infected male participants.

Table 2.

Descriptive data pertaining to the acoustic parameters grouped by health status in the male participants

Parameters	Healthy		Patient	
	Mean (SD)	Range	Mean (SD)	Range
F0 (Hz)	140.61 (24.72)	107.93-206.55	146.11 (26.62)	109.51-210.80
F0 SD (Hz)	8.19 (7.08)	1.96-28.10	10.73 (8.76)	2.20-37.31
Jitter %	0.43 (0.15)	0.22-1.04	0.95 (0.96)	0.36-5.44
Shimmer %	3.28 (1.13)	1.17-6.59	4.66 (2.52)	1.57-13.20
HNR (dB)	46.74 (6.42)	28.89-58.89	26.79 (6.27)	16.41-38.60
CPP (dB)	26.55 (2.69)	19.51-31.88	24.17 (3.26)	17.89-30.98
H1H2 (dB)	3.38 (3.79)	-2.5-11.19	7.23 (2.89)	2.11-13.19
MPT (s)	14.69 (4.35)	6.69-24.92	7.02 (2.05)	3.95-13.60

Table 3 presents the mean, standard deviation and range of all the acoustic parameters in the healthy and infected female participants.

Table 3.

Descriptive data pertaining to the acoustic parameters grouped by health status in the female participants

Parameters	Healthy		Patient	
	Mean (SD)	Range	Mean (SD)	Range
F0 (Hz)	209.99 (23.20)	152.79-261.19	207.41 (31.73)	166.55-327.50
F0 SD (Hz)	8.87 (7.67)	2.17-37.20	16.70 (9.04)	4.43-43.33
Jitter %	0.41 (0.14)	0.16-0.84	1.181 (1.18)	0.35-5.58
Shimmer %	3.78 (1.68)	1.39-9.82	5.12 (3.67)	1.43-18.51
HNR (dB)	53.42 (4.77)	43.83-64.99	30.36 (6.73)	17.05-41.47
CPP (dB)	25.13 (2.67)	20.33-31.09	22.22 (2.96)	15.85-29.09
H1H2 (dB)	8.27 (3.68)	1.72-14.96	10.06 (2.76)	4.65-14.18
MPT (s)	13.55 (4.02)	5.47-26.52	6.21 (2.50)	2.15-10.97

A two-way ANOVA was performed to separately examine the effect of status and gender on F0, CPP, HNR and H1H2. The analysis showed that gender has a significant effect on F0 values (F_1 ,

$_{130} = 203.532$; $p < 0.001$; $\eta_g^2 = 0.610$); however, there was neither a significant difference between F0 values in the healthy and infected participants ($F_{1, 130} = 0.146$; $p > 0.001$; $\eta_g^2 = 0.001$), nor a significant interaction between status and gender ($F_{1, 130} = 0.771$; $p > 0.001$; $\eta_g^2 = 0.006$). When CPP was considered the dependent variable and status and gender the independent variables, the analysis revealed a significant dependence on status ($F_{1, 130} = 26.741$; $p < 0.001$; $\eta_g^2 = 0.171$) and gender ($F_{1, 130} = 10.772$; $p < 0.001$; $\eta_g^2 = 0.077$). Nonetheless, no significant interaction was observed between status and gender ($F_{1, 130} = 0.273$; $p > 0.001$; $\eta_g^2 = 0.002$). the analysis displayed a significant difference in HNR values between the healthy and infected participants ($F_{1, 130} = 414.303$; $p < 0.001$; $\eta_g^2 = 0.761$) and between the female and male participants ($F_{1, 130} = 24.637$; $p < 0.001$; $\eta_g^2 = 0.159$). No interaction was observed between status and gender ($F_{1, 130} = 2.170$; $p > 0.001$). The analysis also showed that H1H2 values were significantly affected by participants' health status ($F_{1, 130} = 23.794$; $p < 0.001$; $\eta_g^2 = 0.155$) and gender ($F_{1, 130} = 44.180$; $p < 0.001$; $\eta_g^2 = 0.254$). No significant interaction was found between status and gender ($F_{1, 130} = 2.825$; $p > 0.001$; $\eta_g^2 = 0.021$).

Wilcoxon's rank-sum test for jitter ($p = 0.39 > 0.05$; $r = 0.07$), shimmer ($p = 0.68 > 0.05$; $r = 0.035$) and MPT ($p = 0.90 > 0.05$; $r = 0.010$) showed that men's median jitter, shimmer and MPT were not significantly different from women's median jitter, shimmer and MPT, respectively. Nonetheless, the difference in median jitter ($p < 0.05$; $r = 0.657$), shimmer ($p < 0.05$; $r = 0.233$) and MPT ($p < 0.05$; $r = 0.778$) between the healthy participants and the infected was significant. The results of Wilcoxon's rank-sum test for F0SD showed a significant difference between men's and women's median F0SD ($p < 0.05$; $r = 0.175$) and also a difference in the median F0SD between the healthy and infected participants ($p < 0.05$; $r = 0.292$).

Based on the results, MPT ($r = 0.778$), HNR ($\eta_g^2 = 0.761$) and jitter ($r = 0.657$) had the largest effect sizes among all the other parameters. That is, 77.8% of variability in MPT values, 76.1% of the change in HNR values and 65.7% of the change in jitter values can be accounted for the participants' health status. As expected, 61% of the variability in F0 and 29.2% of the variability in F0SD can be interpreted as the effect of gender on these parameters' values. According to Cohen^{42,43}, r values varying more than 0.5 indicate a large effect.

4. Discussion

The aim of this study was to investigate whether acoustic parameters of voice differ significantly between covid-19 patients and healthy participants. Fundamental frequency (F0) and its variations (F0SD), fundamental frequency perturbation measures (i.e. jitter and shimmer), harmonics-to-noise ratio (HNR), difference between the first two harmonic amplitudes (H1-H2), maximum phonation time (MPT) and cepstral peak prominence (CPP) were thus measured. These parameters can delineate different aspects of vocal apparatus dysfunction in voice production including irregularity and aperiodicity in vocal fold vibration, airflow insufficiency, increased noise and signal perturbations.^{44,45, 23}

Except F0, all the other acoustic parameters were significantly different between the experimental and control groups.

The results obtained in this study showed a notable difference in fundamental frequency variation (F0SD) between the healthy and infected participants, which could stem from tremor and insufficient control over laryngeal muscles in the experimental group.^{23,46} An increase in jitter and shimmer was also observed in both female and male patients. The uneven weighting of the vocal folds, which occurs due to inflammation or degeneration of the vocal fold tissues⁴⁷ as a result of recurrent dry coughs, could explain the higher values of jitter and shimmer in the experimental group.

The present study also revealed a decrease in both HNR and CPP values in COVID-19 patients. A decline in these parameters is an indication of increased spectral noise in patients' voices, which consequently led to breathier voice in the experimental group.^{12,48} Moreover, many studies have shown that an increase in H1H2 could be considered one of the acoustic indicators of breathiness^{49,50}, especially in pathological voices.⁵¹ The considerable growth in the value of the H1H2 parameter is in line with these findings. Air leakage and incomplete vocal fold closure, which may result from the trauma of vocal folds⁵² during recurrent coughing, may have contributed to the lowered values of HNR and CPP and breathiness in patients with COVID-19. During coughing, the mechanical forces of contact pressure are remarkably larger than in normal phonation⁵³, which may cause vocal fold injuries. Vomiting, as another symptom of coronavirus, can also give rise to injuries of the vocal folds because of the mechanical force of the gag reflex⁵⁴ and the acidity of the gastric content, which rises up to the throat and irritated the tissues.⁵⁴

Previous studies have shown more aperiodicity in pathological voices with an increase in voice break numbers.^{23,16} According to the present findings, the occurrence of voice break is almost rare in healthy participants, but in the experimental group, it had an increased incidence. This finding also confirms the voice dysfunction and the possible injury in vocal folds.

As shown by the results, the MPT is significantly below the normative data in the experimental group. The phonation duration is strongly correlated with lung volume. As noted earlier, this disease has certain effects on the lungs, which accordingly cause the airflow insufficiency for continuation of voice. Moreover, the inadequate closure of vocal folds in pathological larynx generally reduces MPT due to the leakage of through rima glottidis.^{55,44,16}

5. Conclusion

This study revealed significantly higher values of F0SD, jitter, shimmer, H1H2 and voice break numbers in COVID-19 patients in comparison with the control group. The values of HNR, CPP, and MPT were significantly lower in the experimental group. Changes in MPT demonstrated that these patients suffer mostly from airflow insufficiency due to the involvement of the lungs, which was not far from expectation. The other changes demonstrated some laryngological involvement in patients, since they showed higher aperiodicity, irregularity and signal perturbation and also increased levels of noise in the patients' voice in comparison with the control group.

References

1. Rothan HA, Byrareddy SN. The epidemiology and pathogenesis of coronavirus disease (COVID-19) outbreak. *J Autoimmun.* 2020;(February):102433. doi:10.1016/j.jaut.2020.102433
2. Yuki K, Fujiogi M, Koutsogiannaki S. COVID-19 pathophysiology : A review. *Clin Immunol.* 2020;215(January). doi:10.1016/j.clim.2020.108427
3. Kallvik E, Toivonen L, Peltola V, Kaljonen A, Simberg S. Respiratory Tract Infections and Voice Quality in 4-Year-old Children in the STEPS Study. *J Voice.* 2019;33(5):801.e21-801.e25. doi:10.1016/j.jvoice.2018.01.021
4. Lechien JR, Chiesa-Estomba CM, Cabaraux P, et al. Features of Mild-to-Moderate COVID-19 Patients with Dysphonia. *J Voice.* 2020. doi:10.1016/j.jvoice.2020.05.012
5. Parsa V, Jamieson DG. Acoustic Discrimination of Pathological Voice. *J Speech, Lang Hear Res.* 2001;44(2):327-339. doi:10.1044/1092-4388(2001)027
6. Brockmann M, Drinnan MJ, Storck C, Carding PN. Reliable jitter and shimmer measurements in voice clinics: The relevance of vowel, gender, vocal intensity, and fundamental frequency effects in a typical clinical task. *J Voice.* 2011;25(1):44-53. doi:10.1016/j.jvoice.2009.07.002
7. Dejonckere PH, Bradley P, Clemente P, et al. A basic protocol for functional assessment of voice pathology, especially for investigating the efficacy of (phonosurgical) treatments and evaluating new assessment techniques: Guideline elaborated by the Committee on Phoniatrics of the European Laryngology. *Eur Arch Oto-Rhino-Laryngology.* 2001;258(2):77-82. doi:10.1007/s004050000299
8. Lovato A, De Colle W, Giacomelli L, et al. Multi-Dimensional Voice Program (MDVP) vs Praat for Assessing Euphonic Subjects: A Preliminary Study on the Gender-discriminating Power of Acoustic Analysis Software. *J Voice.* 2016;30(6):765.e1-765.e5. doi:10.1016/j.jvoice.2015.10.012
9. Heman-Ackah YD, Heuer RJ, Michael DD, et al. Cepstral peak prominence: A more reliable measure of dysphonia. *Ann Otol Rhinol Laryngol.* 2003;112(4):324-333. doi:10.1177/000348940311200406
10. Watts CR, Awan SN, Maryn Y. A Comparison of Cepstral Peak Prominence Measures From Two Acoustic Analysis Programs. *J Voice.* 2017;31(3):387.e1-387.e10. doi:10.1016/j.jvoice.2016.09.012
11. Watts CR, Awan SN, Lambert E. Spectral / Cepstral Acoustic Measures Differentiate Hypofunctional from Normal Speakers Purpose.
12. Fraile R, Godino-llorente JJ. Cepstral peak prominence : A comprehensive analysis. *Biomed Signal Process Contorl.* 2014;14:42-54. doi:10.1016/j.bspc.2014.07.001
13. Awan SN, Solomon NP, Helou LB, Stojadinovic A. Spectral-Cepstral Estimation of Dysphonia Severity : External Validation. *Ann Otol Rhinol Laryngol.* 2013;122(1):40-48.

doi:10.1177/000348941312200108

14. Hillenbrand J, Cleveland RA, Erickson RL. Acoustic correlates of breathy vocal quality. *J Speech Hear Res.* 1994;37(4):769-778. doi:10.1044/jshr.3704.769
15. Keating P, Garellek M, Kreiman J. Acoustic properties of different kinds of creaky voice. *ICPhS 2015.* 2015;(1):2-7.
16. Karlsen T, Sandvik L, Heimdal JH, Aarstad HJ. Acoustic Voice Analysis and Maximum Phonation Time in Relation to Voice Handicap Index Score and Larynx Disease. *J Voice.* 2020;34(1):161.e27-161.e35. doi:10.1016/j.jvoice.2018.07.002
17. Schindler A, Mozzanica F, Vedrody M, Maruzzi P, Ottaviani F. Correlation between the Voice Handicap Index and voice measurements in four groups of patients with dysphonia. *Otolaryngol - Head Neck Surg.* 2009;141(6):762-769. doi:10.1016/j.otohns.2009.08.021
18. HOLLIEN H. Some laryngeal correlates of vocal pitch. *J Speech Hear Res.* 1960;3(1):52-58. doi:10.1044/jshr.0301.52
19. Titze IR. *Principles of Voice Production.* Prentice Hall; 1994.
<https://books.google.com/books?id=m48JAQAAMAAJ>.
20. Seikel JA, Drumright DG, Seikel P. *Essentials of Anatomy & Physiology for Communication Disorders.* Delmar Cengage Learning; 2013.
<https://books.google.com/books?id=wD-9MgEACAAJ>.
21. Patel RR, Harris MS, Halum SL. Objective Voice Assessment. In: Sataloff RT, ed. *Sataloff's Comprehensive Textbook of Otolaryngology Head & Neck Surgery: Laryngology (Vol. 4).* New Delhi, London, Philadelphia, Panama: Jaypee Brothers Medical Publishers (P) Ltd: The health Science Publisher; 2016:155-168.
22. DAVIS SB. Acoustic Characteristics of Normal and Pathological Voices. *Speech Lang.* 1979;1:271-335. doi:10.1016/b978-0-12-608601-0.50010-3
23. Rusz J, Klempíř J, Baborová E, et al. Objective Acoustic Quantification of Phonatory Dysfunction in Huntington's Disease. *PLoS One.* 2013;8(6).
doi:10.1371/journal.pone.0065881
24. Behrman A. *Speech and Voice Science.* 3rd ed. San Diego, CA: Plural Publishing; 2018.
25. Rosa IS. Análise acústica da voz de indivíduos na terceira idade. 2005.
26. Deliyski DD. Acoustic model and evaluation of pathological voice production. In: *Third European Conference on Speech Communication and Technology, EUROSPEECH.* Berlin; 1993:22-25.
27. Hillenbrand JM. Acoustic Analysis of Voice: A Tutorial. *Perspect Speech Sci Orolfac Disord.* 2011;21(2):31. doi:10.1044/ssod21.2.31
28. Boersma P. Accurate short-term analysis of the fundamental frequency and the harmonics-to-noise ratio of a sampled sound. *IFA Proc 17.* 1993;17:97-110.
http://www.fon.hum.uva.nl/paul/papers/Proceedings_1993.pdf.

29. Teixeira JP, Oliveira C, Lopes C. Vocal Acoustic Analysis – Jitter, Shimmer and HNR Parameters. *Procedia Technol.* 2013;9:1112-1122. doi:10.1016/j.protcy.2013.12.124
30. Hillenbrand JM, Houde RA. Acoustic Correlates of Breathless Vocal Quality : Dysphonic Voices and Continuous Speech. *J Speech Hear Res.* 1996;39(2):311-321. doi:10.1044/jshr.3902.311
31. Hanson HM, Chuang ES. Glottal characteristics of male speakers: Acoustic correlates and comparison with female data. *J Acoust Soc Am.* 1999;106(2):1064-1077. doi:10.1121/1.427116
32. Sapienza C, Hoffman-Ruddy B. *Voice Disorders*. 3rd ed. San Diego, CA: Plural Publishing; 2018.
33. Boersma P, Weenink D. Praat: doing phonetics by computer. 2020. www.praat.org.
34. Omori K. Diagnosis of voice disorders. *Japan Med Assoc J.* 2011;54(4):248-253.
35. Organization WH. *Clinical Management of Severe Acute Respiratory Infection When Novel Coronavirus (2019-NCoV) Infection Is Suspected: Interim Guidance, 28 January 2020*. World Health Organization; 2020.
36. Laver J, Hiller S, Beck JM. Acoustic waveform perturbations and voice disorders. *J Voice.* 1992;6(2):115-126. doi:10.1016/S0892-1997(05)80125-0
37. Shue Y-L, Keating P, Vicenik C. VOICESAUCE: A program for voice analysis. *J Acoust Soc Am.* 2009;126(4):2221. doi:10.1121/1.3248865
38. Kawahara H, Masuda-Katsuse I, Cheveigné A [de. Restructuring speech representations using a pitch-adaptive time–frequency smoothing and an instantaneous-frequency-based F0 extraction: Possible role of a repetitive structure in sounds] Speech files available. See <http://www.elsevier.nl/locate/specom1>. *Speech Commun.* 1999;27(3):187-207. doi:https://doi.org/10.1016/S0167-6393(98)00085-5
39. Krom G De. A Cepstrum-Based Technique for Determining a Harmonics-to-Noise Ratio in Speech Signals. *J Speech Hear Res.* 1993;36(April 1993):254-266. doi:10.1044/jshr.3602.254
40. Iseli M, Shue Y, Alwan A. Age , sex , and vowel dependencies of acoustic measures related to the voice source a). *J Acoust Soc Am.* 2007;121:2283-2295. doi:10.1121/1.2697522
41. R Core Team. R: A Language and Environment for Statistical Computing. 2020. <https://www.r-project.org/>.
42. Cohen J. Statistical Power Analysis. *Curr Dir Psychol Sci.* 1992;1(3):98-101. doi:10.1111/1467-8721.ep10768783
43. Cohen J. *Statistical Power Analysis for the Behavioral Sciences*. 2nd ed. Hillside, NJ: Lawrence Erlbaum Associates; 1988.
44. Yanagihara N, Koike Y, Von Leden H. Phonation and respiration. Function study in normal subjects. *Folia Phoniatr (Basel).* 1966;18(5):323—340.

<http://europepmc.org/abstract/MED/5959236>.

45. PTACEK PH, SANDER EK. Breathiness and Phonation Length. *J Speech Hear Disord.* 1963;28(3):267-272. doi:10.1044/jshd.2803.267
46. Zwirner P, Murry T, Woodson GE. Phonatory function of neurologically impaired patients. *J Commun Disord.* 1991;24(4):287-300. doi:10.1016/0021-9924(91)90004-3
47. Ferrand CT. *Voice Disorders: Scope of Theory and Practice*. Boston: Allyn and Bacon; 2012.
48. Hartl DM, Hans S, Vaissière J, Riquet M, Brasnu DF. Objective voice quality analysis before and after onset of unilateral vocal fold paralysis. *J Voice.* 2001;15(3):351-361. doi:10.1016/S0892-1997(01)00037-6
49. Klatt DH, Klatt LC. *Analysis , Synthesis , and Perception of Voice Quality Variations among Female and Male Talkers*. Vol 87.; 2014.
50. Bickley C. Acoustic analysis and perception of breathy vowels. *MIT Res Lab Electron Speech Commun Gr Work Pap.* 1982;1:71-81.
51. De Krom G. Some spectral correlates of pathological breathy and rough voice quality for different types of vowel fragments. *J Speech Hear Res.* 1995;38(4):794-811. doi:10.1044/jshr.3804.794
52. Dogan M, Eryuksel E, Kocak I. Subjective and Objective Evaluation of Voice Quality in Patients With Asthma. 2007;21(2):224-230. doi:10.1016/j.jvoice.2005.11.003
53. Hess MM, Verdolini K, Bierhals W, Mansmann U, Gross M. Endolaryngeal contact pressures. *J Voice.* 1998;12(1):50-67. doi:10.1016/S0892-1997(98)80075-1
54. Datta R, Datta K, Venkatesh MD. Laryngopharyngeal Reflux : Larynx on Fire. *Med journal, Armed Forces India.* 2010;66(3):245-248. doi:10.1016/S0377-1237(10)80049-8
55. Ortega J, Cassinello N, Dorcaratto D. Computerized acoustic voice analysis and subjective scaled evaluation of the voice can avoid the need for laryngoscopy after thyroid surgery. *Surgery.* 145(3):265-271. doi:10.1016/j.surg.2008.11.002